

(19) World Intellectual Property  
Organization  
International Bureau



(43) International Publication Date  
18 November 2004 (18.11.2004)

PCT

(10) International Publication Number  
**WO 2004/098574 A1**

- (51) International Patent Classification<sup>7</sup>: **A61K 9/51**
- (21) International Application Number:  
PCT/GB2004/001931
- (22) International Filing Date: 5 May 2004 (05.05.2004)
- (25) Filing Language: English
- (26) Publication Language: English
- (30) Priority Data:  
0310300.9 6 May 2003 (06.05.2003) GB
- (71) Applicant (for all designated States except US): **THE QUEEN'S UNIVERSITY OF BELFAST** [GB/GB]; University Road, Belfast BT7 1NN (GB).
- (72) Inventors; and
- (75) Inventors/Applicants (for US only): **CRAIG, Duncan, Q., M.** [GB/GB]; 42 Marlborough Park North, Belfast BT9 6HJ (GB). **MC NALLY, John, Anthony** [IE/GB]; 11c Lenny's Road, Derryadd, Lurgan, Co Armagh BT66 6QS (GB).
- (74) Agent: **MURGITROYD & COMPANY**; Scotland House, 165-169 Scotland Street, Glasgow G5 8PL (GB).
- (81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.
- (84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).
- Published:
- with international search report
  - before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments
- For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

(54) Title: **NANOCOMPOSITE DRUG DELIVERY COMPOSITION**

(57) Abstract: The invention relates to a drug delivery composition comprising an active ingredient and a biologically inert material wherein the biologically inert material is a nanocomposite material. Preferably the biologically inert material is a polymer-clay nanocomposite comprising up to about 40% by weight of nano-sized (1-1000nm) clay particles dispersed in a polymeric material. The active ingredient may be dispersed in the nanocomposite material or absorbed thereto.

WO 2004/098574 A1

## 1                   **Nanocomposite Drug Delivery Composition**

2

3   The present invention relates to the use of a  
4   nanocomposite material in drug delivery  
5   compositions.

6

7   It is well recognised that there are a number of  
8   circumstances whereby it is desirable to disperse a  
9   drug in a biologically inert matrix in the  
10  preparation of a final dosage form. For example,  
11  the incorporation of drugs and bioactive molecules  
12  into polymeric matrices (eg implants, solid  
13  dispersions) has attracted considerable interest as  
14  a means of improved drug delivery. Similarly, drug  
15  or bioactive-loaded microspheres and nanospheres  
16  have received considerable attention. Various drug  
17  delivery compositions comprise modified release  
18  systems whereby the drug is released at a controlled  
19  rate so as to optimise biological activity and  
20  therapeutic effect of the drug (eg controlled  
21  release oral drug delivery systems). Another  
22  example is the use of drug-loaded medical devices,  
23  whereby polymeric devices such as stents may contain  
24  antibiotics or anticoagulants for purposes such as  
25  the prevention of microbial growth. A further  
26  example is the use of tissue engineering scaffolds,  
27  whereby growth factors may be incorporated into a  
28  polymeric matrix to optimise cell growth on that  
29  matrix. In all cases it is necessary to produce  
30  systems that not only release the drug at an  
31  appropriate rate but also have suitable mechanical  
32  properties for the particular application.

1  
2 Nanocomposites are materials that consist of  
3 particles of one compound with a mean diameter in  
4 the nano-size range (1-1000nm) dispersed throughout  
5 another material, commonly a modified inorganic clay  
6 dispersed within an organic polymer. These polymer-  
7 clay nanocomposites (PCNs) possess advantageous  
8 properties compared to the polymer alone such as  
9 increased mechanical strength, reduced gaseous  
10 permeability and higher heat resistance, even though  
11 the quantity of clay may be 5% or less.  
12 Nanocomposite materials have attracted great  
13 interest due to the wide range of alterations in the  
14 properties of the base polymer engendered by the  
15 incorporation of the clays (see for example Schmidt  
16 et al, Current Opin.Solid State Mat.Sci. (2002) 6,  
17 205-212; Choi et al, Chem.Mater. (2002) 14, 2936-  
18 2939; T.J. Pinnavaia and G.W. Beall, "Polymer-clay  
19 nanocomposites", Wiley, Chichester, 2001).  
20 Moreover, they may be manufactured by a range of  
21 techniques using equipment that is well established  
22 and hence are economical to produce (depending on  
23 the choice of materials, although commonly the  
24 materials used are well recognised and inexpensive).

25  
26 The use, in drug delivery compositions, of  
27 potentially useful matrix materials can be limited  
28 by their mechanical properties. The matrix must  
29 maintain suitable mechanical integrity during the  
30 course of the manufacture process and through its  
31 subsequent handling and use.

32

1 There are many instances whereby the mechanical  
2 properties and / or the release rate of the drugs or  
3 bioactives of known drug delivery compositions are  
4 sub-optimal. The present invention providing as it  
5 does for drug or bioactive-loaded nanocomposites  
6 seeks to address these difficulties.

7

8 Therefore, it is an object of the present invention  
9 to provide a drug delivery composition wherein the  
10 release rate of the drug may be manipulated or  
11 altered so as to be optimised for a given drug or  
12 application.

13

14 It is another object of the invention to provide a  
15 drug delivery composition which is mechanically  
16 suitable for the application to which the drug  
17 delivery composition is to be put and which is  
18 capable of maintaining mechanical integrity  
19 throughout the course of its manufacture, storage,  
20 handling and use as appropriate.

21

22 It is a further object of the invention to provide a  
23 drug delivery composition the manufacture of which  
24 may be carried out economically viable using  
25 equipment that is readily available.

26

27 Accordingly, the present invention provides for the  
28 use of a nanocomposite material in the manufacture  
29 of a drug delivery composition.

30

31 The invention also provides a drug delivery  
32 composition comprising an active ingredient and a

1 biologically inert material wherein the biologically  
2 inert material is a nanocomposite material,  
3 preferably a polymer-clay nanocomposite.

4  
5 Preferably the active ingredient is dispersed  
6 throughout a matrix comprising the biologically  
7 inert material, although the invention also provides  
8 a drug delivery system wherein the active ingredient  
9 is loaded in, or adsorbed to, a vehicle comprising  
10 the biologically inert material.

11  
12 The invention further provides a method of  
13 manufacturing a drug delivery composition comprising  
14 the steps of forming an admixture comprising a  
15 polymer, a clay and an active ingredient and  
16 extruding the admixture to produce an extrudate.

17  
18 The nanocomposite material may comprise up to about  
19 99.9% w/w polymer. Preferably the polymer is  
20 present in an amount of from about 90% w/w to about  
21 99% w/w of the nanocomposite.

22  
23 A wide range of polymers may be employed in the  
24 biologically inert material. Examples of suitable  
25 polymers include polyethylene glycol, poly( $\epsilon$ -  
26 caprolactone), polyvinylpyrrolidone, polylactide,  
27 polyethylene, polystyrene, poly(dimethylsiloxane),  
28 polyaniline, polyester, polyimide, cellulose  
29 derivatives such as hydroxypropyl methyl cellulose  
30 and ethylcellulose, polysaccharides such as  
31 alginates and chitosans, gelatin,  
32 polymethylmethacrylates, silicones,

1 polyacrylonitrile, polyetheretherketone (PEEK),  
2 polyamide, polyurethane, bone and dental cements and  
3 other polymeric prosthetic materials. In addition  
4 materials such as starch and starch derivatives  
5 would also be suitable for use in the inert  
6 material. Materials that are composed of more than  
7 one polymer or a polymer and a plasticizer such as  
8 polyethylene glycol, water or glycerol may also be  
9 included.

10

11 Typically the level of clay within the nanocomposite  
12 may range from less than 1% w/w to about 40% w/w,  
13 although higher levels may be included. Preferably  
14 the amount of clay in the nanocomposite is within  
15 the range of from 1% w/w to 10% w/w of the  
16 nanocomposite material.

17

18 Various clays may be used, either alone or in  
19 combination. Typically silicates may be used that  
20 may be naturally occurring (for example bentonite,  
21 montmorillonite and other smectites) or synthetic  
22 (for example fluorohectorite, fluoromica, layered  
23 double hydroxides).

24

25 The presence of the clay nanoparticles can  
26 dramatically alter the mechanical properties of the  
27 composition of the invention, compared to a  
28 conventional drug delivery vehicle using a polymer-  
29 only matrix, so as to render the system much more  
30 suitable for a particular application. The  
31 mechanical properties of the drug delivery  
32 composition of the invention may be manipulated by

1 suitable choice of nanocomposite component materials  
2 (ie the polymers and clays used) and / or  
3 manufacturing conditions. Furthermore, the rate at  
4 which the composition biodegrades may differ from  
5 that of the polymer alone and may be tailored to  
6 suit a particular active ingredient or therapeutic  
7 application.

8  
9 The teaching of the invention is applicable to all  
10 such methods of nanocomposite manufacture and to all  
11 active ingredients (drugs and bioactive materials  
12 including growth factors, nutraceuticals,  
13 antimicrobials and the like) which can withstand the  
14 manufacturing conditions. Suitable drugs and  
15 bioactives include for example low molecular weight  
16 compounds such as indomethacin and paracetamol,  
17 higher molecular weight compounds such as  
18 hydrocortisone, peptides such as cyclosporin A and  
19 calcitonin and proteins such as insulin and human  
20 recombinant DNase. The manufacturing method used  
21 may be tailored to suit both the performance  
22 requirements of the composition and the lability of  
23 the incorporated bioactive such that degradation may  
24 be minimised by appropriate choice of manufacturing  
25 method.

26

27 The amount of active ingredient employed in the drug  
28 delivery composition of the present invention may  
29 vary depending on the characteristics of each  
30 particular agent. However, the active ingredient  
31 should be employed in an amount which is sufficient  
32 to elicit a therapeutic response upon release from

1 the drug delivery composition. Typically the active  
2 ingredient may be employed in an amount of from less  
3 than 1% to about 40% by weight of the composition.

4

5 A drug delivery composition of the invention may be  
6 prepared according to any known method of  
7 manufacturing nanocomposites which can be modified  
8 so as to facilitate the incorporation of the drugs  
9 or bioactive molecule, for example by melt  
10 extrusion. Other manufacturing methods include *in*  
11 *situ* polymerisation (Paul et al, (2003) Polymer, 44,  
12 443-450), melt intercalation (Lepoittevin et al  
13 (2002) Polymer 43, 4017-4023), sonication (Burnside  
14 and Giannelis (1995) Chemistry of Materials, 7,  
15 1597-1600) sol-gel technology and solution blending.

16

17 In the case of manufacture by melt extrusion, the  
18 various components may be mixed simultaneously  
19 (prior to extrusion) in order to disperse the active  
20 ingredient throughout the nanocomposite material,  
21 although the mixing sequence can influence the  
22 product structure and performance and represents  
23 another means by which the properties and release  
24 characteristics of the composition may be  
25 controlled. Other factors such as the choice of  
26 extrusion screw geometries may influence the  
27 structure and performance of the extrudate. The  
28 drug-loaded nanocomposite extrudate produced may be  
29 ground and then formulated into dosage forms such as  
30 tablets and capsules. In such cases, the person  
31 skilled in the art would appreciate that excipients  
32 such as diluents, lubricants, glidants,



1 disintegrants and the like may be utilised in  
2 preparation of the final dosage form. Further  
3 modifications known in the field of formulation  
4 chemistry, such as the application of enteric or  
5 taste masking coatings to tablets for example, may  
6 be employed.

7

8 Dosage forms categories for which the invention may  
9 be particularly useful include oral drug delivery  
10 systems for modified (fast or slow) release, implant  
11 systems (biodegradable or non-biodegradable),  
12 microspheres and nanoparticles for oral, nasal,  
13 parenteral or topical delivery, medical devices,  
14 suppositories, pessaries, dermatological  
15 preparations, tissue engineering scaffolds.

16

17 The present invention also provides a drug delivery  
18 system wherein an active ingredient loaded in, or  
19 adsorbed to, a vehicle comprising the biologically  
20 inert material, the biologically inert material  
21 being a nanocomposite material. The use of  
22 nanocomposites in the manufacture of drug-loaded  
23 medical devices (for example devices such as stents  
24 containing antibiotics or anticoagulants) affords  
25 similar advantages as those discussed above in terms  
26 of controlled active ingredient delivery and  
27 robustness.

28

29 *Example 1*

30

1 Drug dispersions in polyethylene glycol based  
2 nanocomposites for the oral administration of drugs  
3 were prepared as follows:

4  
5 Polyethylene glycol (PEG) 20000 (Janssen  
6 Pharmaceuticals) was the polymer employed and  
7 Cloisite 30B (Southern Clay Products, USA) was the  
8 clay component. Paracetamol (Sigma, UK) was used as  
9 a model active ingredient. Production of the  
10 nanocomposites was performed by melt extrusion using  
11 a Killon KN-100 (Davis Standard Corporation, USA)  
12 single screw extruder with rod shaped die (38 mm  
13 screw diameter, speed 20-22 rpm, die temp 54-57 °C,  
14 temperature zone 1 50 °C - temperature zone 2 55-60  
15 °C - temperature zone 3 55-60 °C - temperature zone 4  
16 55-60 °C, haul off speed 3-4 m/min, cool to room  
17 temperature). The powders were not subjected to any  
18 treatments prior to extrusion, other than simple  
19 mixing of the three components simultaneously.

20

21 The following combinations were used (all % values  
22 are percentages by weight:

23

- 24 • Paracetamol capsule (number 3, white, gelatin  
25 capsule)
- 26 • 5% paracetamol in PEG (pPEG)
- 27 • paracetamol 5%/Cloisite 30B 4% /PEG 95% (the  
28 drug loaded nanocomposite of the invention)

29

30 The extrudates emerged as cylindrical solid tube-  
31 like structures of approximately 5 mm in diameter.

1 During the processing of pPEG the following readings  
2 were obtained: screw amps: 4; die pressure: 0.1  
3 kg/cm<sup>2</sup>; however when the nanocomposite mixture was  
4 extruded the screw amps and die pressure values  
5 increased to 8 and 0.4 respectively evidencing the  
6 enhanced mechanical strength and resistance of the  
7 nanocomposites. Extrusion conditions were optimised  
8 by initially heating the system to beyond the  
9 melting point of the PEG (circa 60°C) and cooling to  
10 circa 56°C so as to extrude the material when in a  
11 supercooled state thus facilitating rapid  
12 solidification upon extrusion from the equipment.  
13 The nanocomposite extrudates produced were  
14 mechanically robust and could be snapped by manual  
15 application of pressure.

16

17 In testing the release characteristics of each  
18 sample the following dissolution methodology was  
19 used (Copley DIS 8000): USP apparatus 2 - rotating  
20 paddle, 50 rpm; medium - 900 ml deionised water (37  
21 °C ± 0.5 °C); analysis - UV spectrophotometer (243  
22 nm).

23

24 Dissolution properties were measured as follows: A  
25 UV calibration plot from a stock solution of  
26 paracetamol was prepared (100mg in 100ml), with  
27 measurements taken at 249nm. Five samples were used  
28 for each experiment with 10ml removed at appropriate  
29 time intervals and replaced with 10mls 37°C  
30 deionised water. The samples were analysed using UV  
31 measurement at 249nm. Samples were prepared by  
32 breaking the extrudate into approximately 1cm

1 lengths, with a corresponding sample weight of circa  
2 0.3g. For the pPEG samples, samples were taken  
3 every 5 minutes for 30 minutes. For the  
4 nanocomposite composition samples were taken every  
5 20 minutes for 4 hours.

6  
7 The release profiles of the three combinations  
8 tested are shown in Figure 1. The release profile  
9 of the paracetamol nanocomposite of the invention  
10 indicates a slower release rate plateauing at about  
11 60 min compared to rate of release from the  
12 paracetamol capsule which reached a plateau at about  
13 30 min. The release profile of the pPEG sample was  
14 faster than both the drug loaded nanocomposite of  
15 the invention and the paracetamol capsule,  
16 plateauing after about 20 min.

17  
18 The test data indicates that the nanocomposite  
19 system may be used as a controlled release drug  
20 delivery system whereby drug release from the  
21 composition is slowed or otherwise manipulated in  
22 comparison to the non-clay containing system.

23

#### 24 *Example 2*

25

26 A further drug delivery composition, in the form of  
27 a drug loaded polyurethane nanocomposite for use in  
28 an insert device, was prepared as follows:

29

30 The polymer / clay / drug composition was  
31 thermoplastic polyurethane (95 %) / Cloisite 30B (4  
32 %) / hydrocortisone (1 %). The mixture of

1 constituents was extruded using a Collin GmbH twin  
2 screw extruder (Model ZK 25), adapter temperature  
3 190 °C, die temperature 19 °C, melt temperature 188  
4 °C, melt zones on the extruder were set between 195  
5 °C and 190 °C from the feed end and screw speed was  
6 90 rpm. The mixture was extruded through a cast  
7 film die to produce 200 micron thick, 40 to 50 mm  
8 wide film of the drug loaded nanocomposite.

9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20

1

## 2 CLAIMS

3

4 1. A drug delivery composition comprising an active  
5 ingredient and a biologically inert material  
6 wherein the biologically inert material is a  
7 nanocomposite material.

8

9 2. A drug delivery composition according to Claim 1  
10 wherein the active ingredient is dispersed  
11 throughout a matrix comprising the biologically  
12 inert material.

13

14 3. A drug delivery composition according to either  
15 of Claims 1 and 2 wherein the nanocomposite is a  
16 polymer-clay nanocomposite.

17

18 4. A drug delivery composition according to any one  
19 of Claims 1 to 3 wherein the nanocomposite  
20 comprises at least one polymer selected from the  
21 group consisting of polyethylene glycol, poly( $\epsilon$ -  
22 caprolactone), polyvinylpyrrolidone, polylactide,  
23 polyethylene, polystyrene,  
24 poly(dimethylsiloxane), polyaniline, polyester,  
25 polyimide, cellulose derivatives such as  
26 hydroxypropyl methyl cellulose and ethylcellulose,  
27 polysaccharides such as alginates and chitosans,  
28 gelatin, polymethylmethacrylates, silicones,  
29 polyacrylonitrile, PEEK, polyamide, polyurethane,  
30 bone and dental cements, starch and starch  
31 derivatives.

32

1 5. A drug delivery composition according to any one  
2 of Claims 1 to 4 wherein the nanocomposite  
3 comprises at least one clay selected from the  
4 group consisting of bentonite, montmorillonite,  
5 fluorohectorite, fluoromica and layered double  
6 hydroxides.

7  
8 6. A drug delivery composition according to any one  
9 of Claims 1 to 5 wherein the amount of clay  
10 within the nanocomposite is up to 40% w/w of the  
11 nanocomposite material.

12  
13 7. A drug delivery composition according to any one  
14 of Claims 1 to 5 comprising at least one active  
15 ingredient selected from the group consisting of  
16 indomethacin, paracetamol, hydrocortisone,  
17 cyclosporin A, calcitonin, insulin and human  
18 recombinant DNase.

19  
20 8. A drug delivery composition according to any one  
21 of Claims 1 to 7 wherein the active ingredient is  
22 present in an amount of up to 40% by weight of  
23 the drug delivery composition.

24  
25 9. A drug delivery system wherein an active  
26 ingredient loaded in, or adsorbed to, a vehicle  
27 comprising the biologically inert material  
28 wherein the biologically inert material is a  
29 nanocomposite material.

30  
31 10. A drug delivery system where the nanocomposite  
32 material is a polymer-clay nanocomposite.

- 1  
2 11. A drug delivery system according to either of  
3 Claims 9 and 10 wherein the nanocomposite  
4 comprises at least one polymer selected from the  
5 group consisting of polyethylene glycol, poly( $\epsilon$ -  
6 caprolactone), polyvinylpyrrolidone, polylactide,  
7 polyethylene, polystyrene,  
8 poly(dimethylsiloxane), polyaniline, polyester,  
9 polyimide, cellulose derivatives such as  
10 hydroxypropyl methyl cellulose and ethylcellulose,  
11 polysaccharides such as alginates and chitosans,  
12 gelatin, polymethylmethacrylates, silicones,  
13 polyacrylonitrile PEEK, polyamide, polyurethane,  
14 bone and dental cements, starch and starch  
15 derivatives.  
16
- 17 12. A drug delivery system according to any one of  
18 Claims 9 and 11 wherein the nanocomposite  
19 comprises at least one clay selected from the  
20 group consisting of bentonite, montmorillonite,  
21 fluorohectorite, fluoromica and layered double  
22 hydroxides.  
23
- 24 13. A drug delivery system according to any one of  
25 Claims 9 to 12 wherein the amount of clay within  
26 the nanocomposite is up to 40% w/w of the  
27 nanocomposite.  
28
- 29 14. A drug delivery system according to any one of  
30 Claims 9 to 13 comprising at least one active  
31 ingredient selected from the group consisting of  
32 indomethacin, paracetamol, hydrocortisone,



1        cyclosporin A, calcitonin, insulin and human  
2        recombinant DNase.

3

4        15. A drug delivery system according to any one of  
5        Claims 9 to 14 wherein the active ingredient is  
6        present in an amount of up to 40% by weight of  
7        the drug delivery system.

8

9        16. A method of manufacturing a drug delivery  
10       composition comprising the steps of forming an  
11       admixture comprising a polymer, a clay and an  
12       active ingredient and extruding the admixture to  
13       produce an extrudate.

14

15       17. A drug delivery composition as defined in any  
16       one of Claims 1 to 8 when produced by a method  
17       according to Claim 16.

18

19       18. A drug delivery composition substantially as  
20       hereinbefore described.

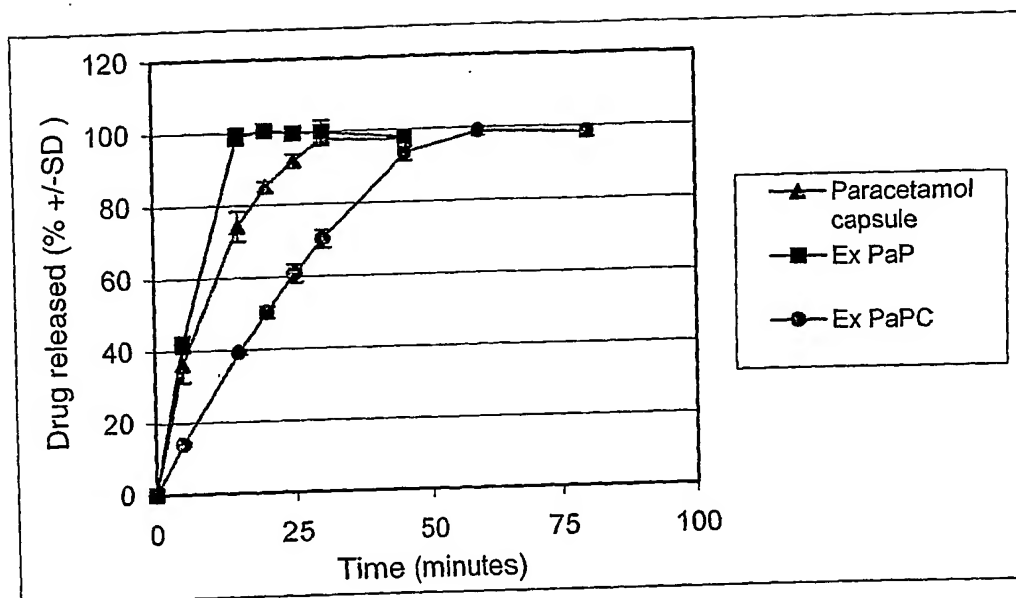
21

22

23

24

1 / 1



- ▲ paracetamol capsule
- paracetamol in PEG (pPEG)
- paracetamol loaded nanocomposite of the invention

Figure 1.

## INTERNATIONAL SEARCH REPORT

International Application No

PCT/GB2004/001931

## A. CLASSIFICATION OF SUBJECT MATTER

IPC 7 A61K9/51

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data, PAJ, MEDLINE, EMBASE, BIOSIS, CHEM ABS Data

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 97/13503 A (SELVARAJ ULAGARAJ ; MESSING GARY L (US); PENN STATE RES FOUND (US)) 17 April 1997 (1997-04-17) examples 2-5 claims 1,2,4,7,9,15,22 -----	1-18
X	US 2002/164482 A1 (AU MING ET AL) 7 November 2002 (2002-11-07) paragraphs '0006!', '0007!', '0087!', '0090!', '0146!', '0159! claims 1,2,4 -----	1-18
X	US 5 683 719 A (NEWTON JOHN MICHAEL) 4 November 1997 (1997-11-04) example 1 claims 1-3,8,9 ----- -/--	16-18

☒ Further documents are listed in the continuation of box C.☒ Patent family members are listed in annex.

## \* Special categories of cited documents :

- \*A\* document defining the general state of the art which is not considered to be of particular relevance
- \*E\* earlier document but published on or after the international filing date
- \*L\* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- \*O\* document referring to an oral disclosure, use, exhibition or other means
- \*P\* document published prior to the international filing date but later than the priority date claimed

\*T\* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

\*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

\*Y\* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

\*G\* document member of the same patent family

Date of the actual completion of the international search

13 October 2004

Date of mailing of the international search report

22/10/2004

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,  
Fax: (+31-70) 340-3016

Authorized officer

Hedegaard, A

## INTERNATIONAL SEARCH REPORT

International Application No  
PCT/GB2004/001931

## C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
------------	--	-----------------------

P,X	CYPES S H ET AL: "Organosilicate-polymer drug delivery systems: controlled release and enhanced mechanical properties" JOURNAL OF CONTROLLED RELEASE, ELSEVIER SCIENCE PUBLISHERS B.V. AMSTERDAM, NL, vol. 90, no. 2, 24 June 2003 (2003-06-24), pages 163-169, XP004431309 ISSN: 0168-3659 abstract -----	1-18
-----	---	------

A	US 2003/065355 A1 (WEBER JAN) 3 April 2003 (2003-04-03) the whole document -----	1-18
---	---	------

A	WO 00/34393 A (EASTMAN CHEM CO) 15 June 2000 (2000-06-15) the whole document -----	1-18
---	---	------

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/GB2004/001931

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
WO 9713503	A	17-04-1997	EP 0862420 A1 WO 9713503 A1	09-09-1998 17-04-1997
US 2002164482	A1	07-11-2002	US 6344271 B1 US 2003012952 A1 US 2003012953 A1 US 2002160190 A1 US 2002160191 A1 US 2002168522 A1 US 2002172826 A1 US 2002170593 A1 US 2002176987 A1 US 2003207112 A1 US 2004170820 A1 US 2004067355 A1 US 6716525 B1 US 2004161949 A1 US 2004180203 A1 US 2002051883 A1 US 2002079476 A1	05-02-2002 16-01-2003 16-01-2003 31-10-2002 31-10-2002 14-11-2002 21-11-2002 21-11-2002 28-11-2002 06-11-2003 02-09-2004 08-04-2004 06-04-2004 19-08-2004 16-09-2004 02-05-2002 27-06-2002
US 5683719	A	04-11-1997	AT 151283 T AU 653372 B2 AU 8909691 A CA 2096733 A1 DE 69125619 D1 DE 69125619 T2 EP 0559813 A1 ES 2101082 T3 FI 932320 A WO 9209270 A1 GB 2249957 A , B HU 65756 A2 JP 6502636 T NO 931859 A ZA 9109185 A	15-04-1997 29-09-1994 25-06-1992 23-05-1992 15-05-1997 11-09-1997 15-09-1993 01-07-1997 09-07-1993 11-06-1992 27-05-1992 28-07-1994 24-03-1994 21-07-1993 30-09-1992
US 2003065355	A1	03-04-2003	CA 2456918 A1 CA 2457189 A1 EP 1429833 A2 EP 1429683 A2 WO 03049795 A2 WO 03026532 A2 US 2003093107 A1	19-06-2003 03-04-2003 23-06-2004 23-06-2004 19-06-2003 03-04-2003 15-05-2003
WO 0034393	A	15-06-2000	AU 758915 B2 AU 1935500 A DE 69910617 D1 DE 69910617 T2 EP 1141136 A1 JP 2002531675 T WO 0034393 A1 US 6417262 B1 US 6384121 B1	03-04-2003 26-06-2000 25-09-2003 17-06-2004 10-10-2001 24-09-2002 15-06-2000 09-07-2002 07-05-2002

**THIS PAGE BLANK (USPTO)**